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# A Review of Atomic-Force Microscopy in Skin Barrier Function Assessment

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Skin barrier function (SBF) disorders are a class of pathologies that affect a significant portion of the world population. These disorders cause skin lesions with intense itch, impacting patients' physical and psychological well-being as well as their social functioning. It is in the interest of patients that their disorder be monitored closely while under treatment to evaluate the effectiveness of the ongoing therapy and any potential adverse reactions. Symptom-based assessment techniques are widely used by clinicians; however, they carry some limitations. Techniques to assess skin barrier impairment are critical for understanding the nature of the disease and for helping personalize treatment. This review recalls the anatomy of the skin barrier and describes an atomic-force microscopy approach to quantitatively monitor its disorders and their response to treatment. We review a panel of studies that show that this technique is highly relevant for SBF disorder research, and we aim to motivate its adoption into clinical settings.

**Keywords:** Atomic-force microscopy, Atopic dermatitis, Corneocyte morphology, Skin barrier function

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## INTRODUCTION

Skin barrier function (SBF) disorders are a common class of pathologies that present a major burden on global health. Atopic dermatitis (AD) is an SBF disorder of particular interest, affecting roughly 790 million people (10 % of adults and 20% of children globally [Silverberg et al, 2021]). It is an

inflammatory skin disease that causes eczematous lesions and intense itch (Nutten, 2015). The typical onset of AD is in infancy to early childhood, and its increasing prevalence presents serious concerns (Charman et al, 2004; Nutten, 2015). It is a distressing and chronic condition characterized by skin barrier abnormalities, immune deregulation, cutaneous inflammation, and microbiome alteration. Similar to other SBF disorders, AD is sometimes accompanied by atopic conditions such as food allergies, allergic asthma, and allergic rhino-conjunctivitis.

Its symptoms can be severe enough to traumatize and impair the psychological well-being, development, and social functioning (Rønstad et al, 2018; Urban et al, 2020), not only of the patients but also of their family (Vitrup et al, 2022). Moreover, AD brings a significant economic burden: the total cost per patient with severe AD can reach €15,000 per year (Bieber, 2022).

Although there is no known cure for AD, appropriate treatment can ease symptoms and keep it under control. For moderate to severe AD, physicians have prescribed oral corticosteroids, cyclosporine, or methotrexate (Simpson et al, 2011), which can carry severe dose-dependent side effects, notably nephrotoxicity. Recently, mAbs and Jak inhibitors have emerged as the preferred course for AD management (Dattola et al, 2019). mAbs dupilumab and tralokinumab are approved in the United States and Europe, whereas nemolizumab and lebrikizumab are in clinical trials (Ratchataswan et al, 2021). Jak inhibitors upadactinib and abrocitinib are approved (Kamata and Tada, 2023). However, these treatments represent a significant economic burden, with a lifetime drug cost of up to €268,000 (Zimmermann et al, 2018). Therefore, methods to score the severity of AD—and quantitatively evaluate the efficacy of the interventions—are critical for clinicians and researchers.

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Abbreviations: ACD, allergic contact dermatitis; AD, atopic dermatitis; AFM, atomic-force microscopy; AK, actinic keratosis; CNO, circular nano-object; DTI, dermal texture index; ICD, irritant contact dermatitis; KC, keratinocyte; LoF, loss-of-function; MCI, methylchloroisothiazolinone; MI, methylisothiazolinone; NMF, natural moisturizing factor; OBD, optical beam deflection; OPU, optical pickup unit; PSPD, position-sensitive photodiode; SB, stratum basale; SBF, skin barrier function; SC, stratum corneum; SCORAD, Severity Scoring of Atopic Dermatitis; SG, stratum granulosum; SLS, sodium lauryl sulfate; SS, stratum spinosum; TEWL, transepidermal water loss

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121 Current scoring methods, such as Severity Scoring of  
 122 Atopic Dermatitis (SCORAD) (Kunz et al, 1997), Eczema  
 123 Area and Severity Index (Hanifin et al, 2001; Leshem et al,  
 124 2015), Patient-Oriented Eczema Measure (Charman et al,  
 125 2004), and Investigator global assessment (Futamura et al,  
 126 2016; Simpson et al, 2020, 2011), provide researchers and  
 127 clinicians with well-tested standards to assess AD severity.  
 128 However, they rely on visual observation and interrogation of  
 129 the patients or their parents, which makes subjectivity un-  
 130 avoidable. Moreover, because they are based on symptom-  
 131 atic manifestation of the disease, they cannot be used to study  
 132 its pre or postsymptomatic evolution. Analytical methods  
 133 exist (Drutis et al, 2014; Xing et al, 2017), but these are  
 134 costly, requiring specialized equipment with highly trained  
 135 operators, and have a turnaround time of several days to  
 136 weeks. Because of these limitations, current scoring methods  
 137 could be improved on to make frequent observations, to  
 138 monitor the early onset and evolution of the disease, to  
 139 routinely evaluate the effectiveness of a prescribed treatment,  
 140 or to proactively manage the QOL of the patient in the long  
 141 term.

142 To this end, we recall a method that uses a noninvasive  
 143 skin tape-stripping method for ex vivo analysis. Atomic-force  
 144 microscopy (AFM) analysis of the corneocyte texture provides  
 145 an objective and quantitative metric related to SBF able to  
 146 detect physiological changes before, during, and after the  
 147 SBF disorder is manifest. This review will discuss the forma-  
 148 tion of the stratum corneum (SC) and introduce AFM in the  
 149 field of dermatology. We aim to show that nanotexture  
 150 analysis is a useful tool to study AD and other skin barrier  
 151 dysfunctions, and we hope to motivate its adoption in clin-  
 152 ical, patient-facing use.

## 154 HUMAN SKIN

155 The skin contains 3 distinct layers: epidermis, dermis, and  
 156 subcutis or hypodermis (Montagna and Parakkal, 1974;  
 157 Wong et al, 2016). The epidermis is the outermost barrier and  
 158 protects the body against chemicals, allergens, and patho-  
 159 gens while maintaining balance of fluids with the outside  
 160 environment (Koster, 2009; Simpson et al, 2011). The  
 161 epidermis is divided into 5 layers or strata: SC, stratum luci-  
 162 dum (only present in thick hairless skin [Yousef et al, 2022]),  
 163 stratum granulosum (SG), stratum spinosum (SS), and stratum  
 164 basale (SB) (Fuchs and Raghavan, 2002). The lower strata are  
 165 predominated by keratinocyte (KC) cells, which differentiate  
 166 and migrate upward from the SB to the SS. The KCs are  
 167 connected mechanically by desmosomes and adherens  
 168 junctions (Hwa et al, 2011).

169 When KCs reach the SG, they develop intracellular kera-  
 170 tohyalin granules containing pro-FLG as the precursor protein  
 171 of FLG (Thyssen and Kezic, 2014). The SG is also responsible  
 172 for producing the lipids that complete the skin barrier when  
 173 reaching the SC. At the border between SG and SC, pro-FLG  
 174 is dephosphorylated into FLG monomers. In the SC, the FLG  
 175 monomers aggregate the keratin filaments inside the cell,  
 176 flattening the KCs and creating macrofibrils that mechani-  
 177 cally tether them. The FLG monomers are further hydrolyzed  
 178 to amino acids and their derivatives by proteases, including  
 179 caspase-14, bleomycine hydrolase, and calpain 1. The pro-  
 180 liferation rate of KCs is equal to the desquamation rate of the

181 SC on the outer surface (Engebretsen et al, 2016). When KCs  
 182 reach the SC, they differentiate into corneocytes, losing their  
 183 nucleus and collapsing, to eventually shed off. The entire  
 184 epidermal differentiation process takes approximately 28  
 185 days (Regnier et al, 1993).

## 186 The SC

187 The essential function of the SC is to control water loss and  
 188 protect against stressors, but it also acts as an absorption  
 189 route for environmental compounds (Grandjean, 1990). The  
 190 SC is typically described by a bricks and mortar model of  
 191 corneocytes embedded into lipids. The keratin-filled interior  
 192 of corneocytes is enveloped by cornified lipid layers. The  
 193 cornification process comprises 3 main events: forming an  
 194 intracellular keratin network, assembly of cornified lipid en-  
 195 velopes, and selective degradation of corneodesmosomes  
 196 (Harding et al, 2000).

197 The maturation of corneocytes and desquamation of su-  
 198 perfacial cells are well-controlled processes that depend on  
 199 several parameters such as pH gradient, proteases and their  
 200 inhibitors, and hydration of the SC. The interior of corneo-  
 201 cytes contain components such as lactic acid, various amino  
 202 acids, pyrrolidone carboxylic acid, urocanic acid, and hyal-  
 203 uronic acid. These molecules constitute the natural moistur-  
 204 izing factors (NMFs) that maintain SC hydration and low pH  
 205 to prevent cracking and protect against pathogens (Boireau-  
 206 Adamezyk et al, 2021).

207 The mature corneocyte has a diameter of approximately  
 208 25–35  $\mu\text{m}$  and a surface area of 700–900  $\mu\text{m}^2$ , which in-  
 209 creases as they mature (Evans and Roth, 2014; Naoko et al,  
 210 2013). Structural changes are visible between young and  
 211 aged skin because aged skin is characterized by an increase  
 212 in single-cell surface area ( $753 \pm 120 \mu\text{m}^2$ ;  $n = 14$ )  
 213 compared with young skin (surface area:  $555 \pm 80 \mu\text{m}^2$ ;  $n =$   
 214 10) (Gorzellany et al, 2006). An increase in corneocyte  
 215 roughness and a prominent intercellular gap are also char-  
 216 acteristic of aged skin.

## 217 Skin barrier dysfunction

218 The SBF resides largely in the highly organized lipid lamellae,  
 219 composed of ceramides, free fatty acids, and cholesterol. The  
 220 SBF is commonly determined by measuring transepidermal  
 221 water loss (TEWL). The upkeep of an adequate skin barrier is  
 222 also dependent on the skin's NMF concentration, which is  
 223 essential for skin hydration, desquamation, and plasticity.  
 224 Loss-of-function (LoF) mutations in *FLG* gene are determinant  
 225 of low NMF concentration, but T helper 2-mediated  
 226 inflammation and exposure to skin irritants can also lead to  
 227 reduced NMF levels (Thyssen and Kezic, 2014). The NMF  
 228 concentration can be quantified in vivo or ex vivo by chro-  
 229 matographic or spectrometric methods (Caspers et al, 2001;  
 230 Drutis et al, 2014; Soltanipoor et al, 2018).

## 231 Ex in vivo analysis of SC

232 The most common method to assess SC composition in vivo  
 233 is confocal Raman spectroscopy (Caspers et al, 2001; Drutis  
 234 et al, 2014), which can be used to determine NMF, lipids, and  
 235 keratin concentrations. However, this method requires  
 236 expensive instrumentation with highly trained personnel who  
 237 must convene by the instrument with the patient  
 238 (Riethmüller, 2018). Ex vivo methods involve skin sample  
 240



241 collection and separate analysis of the sample. These  
242 methods allow for repeatability, centralization of analysis,  
243 and better convenience to the patient.

244 A noninvasive way to collect skin tissue is the tape-  
245 stripping method (Lademann et al, 2009). It involves press-  
246 ing a circular adhesive tape for a few seconds onto the sur-  
247 face of the skin and then carefully removing the tape. The  
248 outermost layers of corneocytes adhere to the tape and are  
249 peeled off. On average, depending on SC cohesion, type of  
250 the adhesive tape, and applied pressure, 1 SC layer is  
251 removed per tape, but variability is high. For detailed dis-  
252 cussion on the amount of corneocytes removed, see Jacobi  
253 et al (2005), Keurentjes et al (2021), Simon et al (2023),  
254 and Sølberg et al (2019). Successive peels of the same area  
255 can be used to study corneocytes at different depths of the SC  
256 (Lademann et al, 2009). The skin tape is small (<30 mm in  
257 diameter) and lightweight (<1 g), which makes it practical to  
258 ship to laboratories for centralized analysis.

259 The tape-stripped corneocyte samples can be studied  
260 either morphologically or biochemically. For biochemical  
261 analysis, the tape is soaked in a solvent or buffer to extract the  
262 compound of interest, which is then determined by an  
263 appropriate method (Hulshof et al, 2019; Riethmuller et al,  
264 2015). In dermatological research, the tape-stripping tech-  
265 nique is often used to determine NMF levels in the corneo-  
266 cyte as a biomarker of LoF mutations in *FLG* gene, which is  
267 one of the main risk factors in AD development. Furthermore,  
268 tape-stripped corneocytes have also been used to determine  
269 immunological profiles (Keurentjes et al, 2021).

270 Beyond biochemical assays, tape-stripped corneocytes  
271 lend themselves to morphological characterization. Because  
272 they are affected by the condition of the skin during their 4-  
273 week maturation from the SB, they carry information about  
274 skin abnormalities, which is revealed by imaging. There are 2  
275 main corneocyte imaging methods: scanning electron mi-  
276 croscopy and AFM. Sufficient-resolution scanning electron  
277 microscopy requires a vacuum environment and metal  
278 coating of the sample, which makes it impractical for routine  
279 research and clinical applications. In contrast, AFM can  
280 achieve atomic resolution without the need for vacuum or  
281 special sample preparation. In addition, AFM can probe the  
282 sample's mechanical properties such as elasticity and friction.  
283 Therefore, AFM is an ideal tool to image (Braet et al, 1998;  
284 Fredonnet et al, 2014; Gorzelanny et al, 2006; Kashibuchi  
285 et al, 2002) nanotextures and characterize the mechanical  
286 properties (Fredonnet et al, 2014; Gaikwad et al, 2010; Tang  
287 and Bhushan, 2010) of the corneocyte.

## 289 AFM

### 290 Introduction to AFM

291 AFM has demonstrated its potential in biological science,  
292 affording high-resolution topography of biological samples  
293 under physiological conditions (Danzberger et al, 2018;  
294 Franz et al, 2016; Fredonnet et al, 2014; Gorzelanny et al,  
295 2006; Rankl et al, 2010), used to determine the mechanical  
296 properties of various tissues (Braet et al, 1998; Grandbois  
297 et al, 2000; Hwang et al, 2013); analyze protein structure  
298 (Hansma and Hoh, 1994); and image living cells (Kasas et al,  
299 1993), chromatin structures (Lohr et al, 2007), and biological  
300 membranes (Frederix et al, 2009).

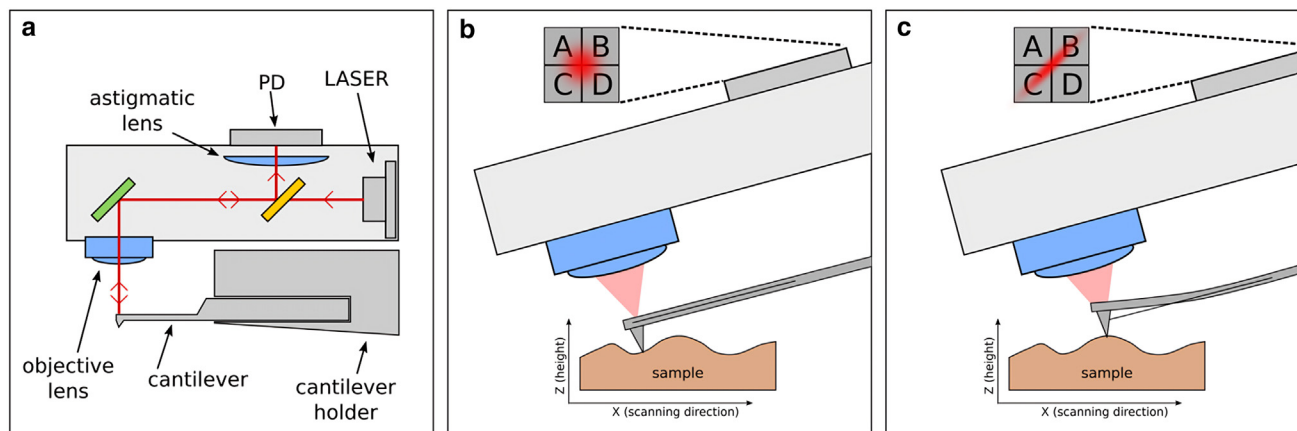
301 AFM is a scanning-probe technique, in which the sample is  
302 fixed on a translation stage that uses piezoelectric transducers  
303 to move the sample on the XY plane. The probe is a micro-  
304 scale cantilever with a sharp tip (apex diameters range from  
305 nm to  $\mu\text{m}$  scale depending on the application) carefully  
306 brought to contact with the sample. The sample surface ex-  
307 erts a force on the tip in the Z direction, which deflects the  
308 cantilever. A raster image of the sample surface topography is  
309 produced by scanning the XY plane and recording the  
310 cantilever deflection as a function of XY position. In con-  
311 ventional AFMs, cantilever deflection is detected by an op-  
312 tical beam deflection (OBD) system, where a laser beam is  
313 focused on the upside of the cantilever and the reflected  
314 beam is made to strike a position-sensitive photodiode  
315 (PSPD). The position of the laser spot on the photodiode is  
316 calculated by comparing the electrical current produced by  
317 each quadrant of the PSPD. The sensitivity is calibrated, so  
318 the probe deflection—and therefore the sample surface  
319 height Z—can be directly calculated from the spot  
320 displacement.

321 The mechanical properties of the sample can also be ob-  
322 tained: if the cantilever stiffness is known, the instantaneous  
323 tip-sample force is deduced from the deflection (Cappella  
324 and Dietler, 1999). From the time-dependent relationship  
325 between the tip-sample force and the Z-displacement,  
326 properties such as elasticity, adhesion force, and energy  
327 dissipation can be derived (Bosco et al, 2013; Braet et al,  
328 1998; Grandbois et al, 2000; Harding et al, 2000; Peñuela  
329 et al, 2018; Riethmüller et al, 2007). The mechanical prop-  
330 erties of the corneocyte have been shown to correlate with  
331 SBF parameters and are likely to have a causative effect on its  
332 reduced function (Haftek et al, 2020). By choosing an AFM  
333 probe with suitable spring constant and tip material, this  
334 measurement can be performed on soft (Dokukin and  
335 Sokolov, 2012), hard (Zeng et al, 2018), and elastic  
336 (Radmacher, 1997) materials.

337 General-purpose laboratory AFMs equip many different  
338 measurement modes with multiple parameters and have a  
339 typical scan rate of 0.5–2 lines per second, which gives  
340 4–17 minutes per image. Usually, this complex system must  
341 be tuned and operated by experienced technicians. More-  
342 over, optical table and thermal/acoustic isolation are needed  
343 for eliminating environmental interference. The whole AFM  
344 setup, including vacuum chambers, delicate optics, elec-  
345 tronics, and surrounding accessories, occupy a large space  
346 ( $\sim 1 \text{ m}^3$ ), bringing the cost of a laboratory AFM up to hun-  
347 dreds of thousands of United States dollars.

### 349 Optical pickup unit-based AFM

350 State-of-the-art AFM has found widespread use in scientific  
351 research, but it has not been adopted into clinical derma-  
352 tology, mainly owing to the cost and complexity of the OBD  
353 system and its need for highly trained operators. Optical  
354 pickup units (OPU) of consumer CD (Compact Disc), DVD  
355 (Digital Versatile Disc), and Blu-ray players have been  
356 repurposed for different scientific applications, such as bio-  
357 sensing (Bache et al, 2013; Bosco et al, 2013, 2011, 2010;  
358 Hwu and Boisen, 2018; Hwu et al, 2013), physical parameter  
359 characterization (Chang et al, 2022; Hwu et al, 2012, 2008;  
360 Liao et al, 2018, 2012), and micro/nanoscale 3-dimensional



**Figure 1. Schematic and operating principle of an OPU-based AFM system.** (a) Simplified schematic of an OPU-based AFM, not to scale. Green, mirror; yellow, beam splitter; and blue, lenses. The circular beam emitted by the integrated LASER is guided to a lens that focuses the light on the back of an AFM cantilever mounted under a commercial OPU. The light is reflected and made to strike an integrated PD through an astigmatic lens. (b) When the cantilever is not deflected, its back remains on the focal plane, and the LASER spot on the PD remains circular. (c) Deflection of the cantilever moves its reflective back outside of the focal plane, causing the LASER spot on the PSPD to be elongated. The deflection of the cantilever is calculated by comparing the current produced by each quadrant of the PD. AFM, atomic-force microscopy; OPU, optical pickup unit; PD, photodetector; PSPD, position-sensitive photodiode.

printing (Chang et al, 2021). Hwu et al (2009, 2008) realized that the OPUs can be used to measure cantilever deflection of the AFM probe (Grey, 2015; Lopez Martinez et al, 2016), replacing the traditional optical system. They constructed an OPU-based AFM (Figure 1) (Hwu et al, 2009, 2007), which senses cantilever deflection without the need for external optics (Liao et al, 2014) and is capable of topographic imaging and calibrated force–displacement imaging (Chang et al, 2022; Liao et al, 2012). Hwu et al (2008) demonstrated that this microscope affords a resolution in air (Hwu et al, 2008) and liquid environments (Hwang et al, 2013; Liao et al, 2013) comparable with conventional AFM.

The optics and electronics of this microscope are integrated in the OPU, a mass-produced inexpensive and robust module, which requires no user tuning. Because OPU sensitivity does not depend on the optical distance between the cantilever and the photodetector, these microscopes are extremely compact. These advantages make OPU-based AFM accessible to clinical settings and allow for the adoption of AFM as a routine diagnostic technique. Hwu et al (XXX) are actively developing open-source hardware and clinic-ready user interfaces that require minimal training to produce nanometer-resolution images (Liao et al, 2022).

### AFM in dermatology

Despite its cost and complexity, traditional AFM has become a principal tool in ex vivo dermatological research (Alsteens et al, 2017; Gaikwad et al, 2010; Irvanimanesh et al, 2017; Kashibuchi et al, 2002; Olejnik and Nowak, 2017; Peñuela et al, 2018; Qassem and Kyriacou, 2019; Rankl et al, 2010; Rinnov et al, 2023; Stylianou, 2017; Tang and Bhushan, 2010) used to analyze the morphology, presence of antibodies, response to irritants and treatments, and mechanical properties of KCs (Boyle et al, 2019; Ramms et al, 2013; Laly et al, 2021; Miroshnikova et al, 2018; Connelly et al, 2021). The fast-advancing field of low-cost OPU-based AFM has opened the opportunity to bring AFM techniques from research into clinics (Liao et al, 2022).

The following section discusses nanotexture analysis, a promising application of AFM, for both AD research and AD health care.

### CORNEOCYTE NANOTEXTURE ANALYSIS

The deep side of tape-stripped corneocytes displays widely varying nanotextures. One of these is a circular nanotexture, commonly found on inflammatory skin and mostly absent in healthy skin (Fredonnet et al, 2014), which is thought to be a result of irregular maturation of corneocytes (Engebretsen et al, 2018a). This circular nanotexture has been called villous-like projections (Naoko et al, 2013; Zeng et al, 2018), bead- or nipple-like elevation (Radmacher, 1997), nanoscale protrusion (Gaikwad et al, 2010), and circular nano-objects (CNOs) (Franz et al, 2016). Because a biological function has not yet been definitively ascertained, this document prefers the term CNO, a strictly phenotypic nomenclature (Riethmüller, 2018).

A dermal texture index (DTI) can be obtained by counting CNOs in nanometer-resolution images of tape-stripped corneocytes. This CNO count was described by Riethmüller (2018) and Franz et al (2016) and thoroughly discussed in Riethmüller (2018). Franz et al (2016) found that skin of healthy subjects had a count of  $24 \pm 21$ , nonlesional skin from AD-affected subjects had a count of  $116 \pm 53$ , and AD lesional skin had a count of  $529 \pm 277$ , regardless of skin pigmentation, making the number of CNOs a quantitative score for AD severity assessment. The research that studies its significance in AD-related conditions can be found in Engebretsen et al (2018a, 2018b), Franz et al (2016), Hulshof et al (2019), Koppes et al (2017), Riethmüller et al (2015), Rüther et al (2021), Soltanipoor et al (2018), Thyssen et al (2020), and Vater et al (2021).

### Nanotexture-based research in AD

Riethmüller et al (2015) investigated corneocyte topography in children with AD and related the measured DTI with *FLG* LoF mutations, TEWL, NMF, and AD severity measured by SCORAD. Subjects with LoF *FLG* mutations (–/– or –/+) had



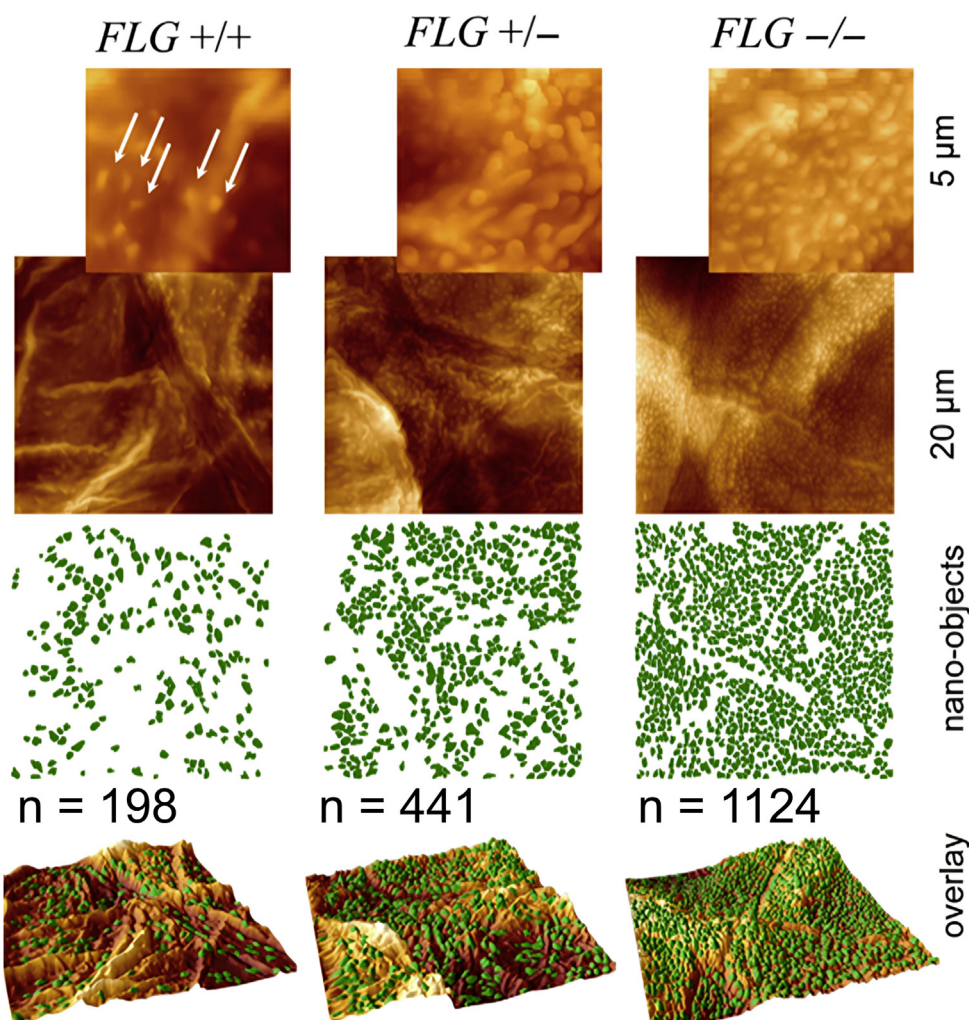


Figure 2. AFM images of skin samples from patients with AD with different FLG mutations. Figure was reprinted from Riethmuller et al (2015) with permission from Elsevier. AD, atopic dermatitis; AFM, atomic-force microscopy.

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considerably higher DTI than wild-type (+/+) subjects with AD (Figure 2), with a correlation to disease severity (SCORAD). A significant (negative) correlation was observed between DTI and NMF. DTI was found to correlate more strongly with NMF ( $r = 0.80$ ) (Riethmuller et al, 2015) than with SCORAD, suggesting that the absence of FLG rather than the presence of inflammation drives the formation of CNOs (villous-like projections in their article).

Nanotexture analysis can also help investigate the correlation between different skin phototypes, immune response biomarkers, and NMF. Hulshof et al (2019) found that immune-response biomarkers (IL-1 $\beta$ , CXCL8, and CCL22, etc) varied significantly between healthy skin and nonlesional AD skin but were independent of skin phototype. In contrast, NMF and CNO-count correlations with AD varied between phototypes.

#### Nanotexture-based SBF assessment

Engebretsen et al (2018a) studied healthy controls and subjects with a history of AD who were asymptomatic or only mildly symptomatic. Their barrier function parameters—TEWL, monomeric FLG levels, and NMF concentrations—were measured as well as their DTIs. A negative correlation between NMF and TEWL was found. The participants with a

history of AD had different nanotexture and lower levels of monomeric FLG and NMF than the healthy controls. In subjects with a history of AD, low levels of monomeric FLG and NMF correlated with the presence of FLG mutations. In a separate study, Engebretsen et al (2016) found that DTI and TEWL were positively correlated in both healthy skin and skin with compromised barrier function.

#### AFM-based research in contact dermatitis

Irritant contact dermatitis (ICD) is a common inflammatory skin disease that occurs when exposed to chemicals such as detergents, alkaline agents, acids, and organic solvents. When skin is exposed to a common detergent, the surface topography of corneocytes changes, as do TEWL and NMF, followed by a significant increase in DTI within 72–96 hours (Koppes et al, 2017; R  ther et al, 2021; Soltanipoor et al, 2018; Vater et al, 2021).

Allergic contact dermatitis (ACD) is clinically similar to ICD. For diagnosis, patch testing, a well-established technique, is used. It is performed by exposing patients to suspected allergens on a small skin area (<1 cm<sup>2</sup>). Inflammation at the application site of a particular substance is considered a positive test and proof of sensitization. However, many allergens often exert irritant properties, which makes

600



601 interpretation of the patch test difficult. To explore DTI as a  
 602 tool to distinguish between ICD and ACD, [Koppes et al](#)  
 603 [\(2017\)](#) studied ex vivo the changes in NMF and corneocyte  
 604 morphology in skin exposed to common allergens: chrom-  
 605 ium, nickel, methylchloroisothiazolinone (MCI), methyl-  
 606 isothiazolinone (MI), and p-phenylenediamine ([Koppes et al](#),  
 607 [2017](#)). As an irritant compound, sodium lauryl sulfate (SLS)  
 608 was included. Elevated DTI was observed when the skin was  
 609 exposed to SLS but also to MCI/MI, which caused a  
 610 remarkable change in NMF levels and had a profound effect  
 611 on corneocyte morphology. They speculate that MCI and MI  
 612 exert skin irritation by damaging the cornified envelope,  
 613 resulting in leakage of NMF.

614 [Soltanipoor et al \(2018\)](#) investigated the effect of different  
 615 skin irritants on corneocyte surface topography. They applied  
 616 acetic acid, n-propanol, SLS, and sodium hydroxide and  
 617 measured several skin parameters 24 and 96 hours after  
 618 application. SLS had the most pronounced impact on cor-  
 619 neocyte surface topography. They concluded that SLS may  
 620 increase the SC pH value and play a predominant role in the  
 621 degradation of FLG into NMF compounds. SLS denatures  
 622 cornified envelope proteins, pro-FLG processing, and des-  
 623 quamatory SC enzymes and may denature NMF compounds.  
 624 The remaining irritants significantly increased the CNO count  
 625 and induced prominent topographical changes such as thin-  
 626 ning of fibers, elongated spots, and wrinkles, which appeared  
 627 after 24 hours and became abundant after 96 hours of  
 628 exposure (most abundant with SLS and n-propanol). CNO  
 629 count was inversely related to NMF levels, which agrees with  
 630 previous studies ([Koppes et al, 2017](#)). This suggests that skin  
 631 texture analysis by AFM is a reliable method to discern true  
 632 allergic reactions from simple irritation ([Corsini and Galbiati](#),  
 633 [2019](#)).

#### 635 AFM-based seasonal change assessment

636 Seasonal factors significantly affect NMF and corneocyte  
 637 morphology ([Engebretsen et al, 2018a](#)). Low humidity and  
 638 low temperature have an adverse effect on SBF and increase  
 639 the risk of dermatitis in general. The degradation of FLG into  
 640 NMF components increases when the ambient humidity de-  
 641 creases, which causes a reduction of NMF level on human  
 642 cheeks ([Scott and Harding, 1986](#)).

643 [Engebretsen et al \(2018a\)](#) studied the seasonal impact on  
 644 skin morphology and NFM levels of 80 healthy subjects.  
 645 Relative to those of summer, winter NMF levels and DTI were  
 646 reduced and elevated, respectively. However, UV exposure  
 647 elevated the DTI and caused changes in the corneocyte  
 648 morphology on the exposed area of the hand and cheek.  
 649 Although low doses of UVB irradiation have positive effects  
 650 on SBF ([Engebretsen et al, 2016](#)), high-dose irradiation of  
 651 UVB negatively affects the corneodesmosomes and intercel-  
 652 lular lipids, leading to decreased skin integrity and skin bar-  
 653 rier impairment ([Engebretsen et al, 2018a](#)). UV reduces the  
 654 SC hydration necessary to maintain NMF levels on the  
 655 cheeks. The reduced skin hydration could initiate FLG  
 656 degradation, altering corneocytes. Other factors that could be  
 657 responsible for alterations on corneocyte morphology are an  
 658 immature cornified envelope and a disorganized cytoskel-  
 659 eton. In contrast to winter, the higher temperature in summer  
 660 stimulates sweating, which could contribute to higher NMF

661 levels. An age dependency of NMF was observed: younger 661  
 662 participants had less NMF than older participants and less 662  
 663 NMF in winter than in summer. This is consistent with pre- 663  
 664 vious studies by high-performance liquid chromatography 664  
 665 ([Engebretsen et al, 2016](#)) and Raman spectroscopy ([Egawa 665](#)  
 666 and [Tagami, 2008](#)). The lower NMF levels in young skin 666  
 667 could be explained by the difference in the level of FLG and 667  
 668 its metabolites: a Japanese study ([Takahashi and Tezuka, 668](#)  
 669 [2004](#)) had previously investigated FLG degradation in those 669  
 670 aged 60–81 years compared with that in those aged 1–10 670  
 671 years. It found that age markedly reduces FLG levels and 671  
 672 markedly increases byproducts of FLG degradation, which 672  
 673 are amino acids and lipids that contribute to NMF. A similar 673  
 674 increase in NMF levels was previously observed in cheek and 674  
 675 arm skin of aged subjects compared with that in young 675  
 676 subjects ([Egawa and Tagami, 2008](#)). Contrary to NFM, many 676  
 677 other SC components (eg, lactates, ceramides, urea) were 677  
 678 lower in aged skin, although the increased NFM levels in 678  
 679 aged subjects could be possibly explained by a larger cell 679  
 680 surface ([Gorzellany et al, 2006](#)) and longer SC transit time 680  
 681 ([Grove, 1983](#); [Mohammed et al, 2012](#)).

#### 682 AFM-based actinic keratosis assessment

683 Actinic keratosis (AK) is a frequent premalignant skin lesion 683  
 684 that develops in light skin phototype (types I and II) subject 684  
 685 to chronic sun exposure ([Keurentjes et al, 2020](#)). Perhaps 685  
 686 motivated by the clinical similarity of inflammatory disease 686  
 687 and keratosis conditions and by the success of AFM in 687  
 688 investigating inflammatory disease, [Keurentjes et al \(2020\)](#) 688  
 689 studied the morphology, DTI, and NFM in lesional AK and 689  
 690 surrounding skin. They found that a change in the general 690  
 691 topography of corneocytes was marked, concomitant with a 691  
 692 marked increase in DTI. They found that DTI decreases and 692  
 693 that NMF increases gradually with distance to the lesion, 693  
 694 remaining affected even in regions with no visible changes. 694  
 695

#### 696 DISCUSSION

697 Although AFM has shown great promise in skin research, 697  
 698 some limitations remain. The high cost and complexity of 698  
 699 traditional AFM have hindered clinical adoption. Further- 699  
 700 more, data acquisition and analysis currently require 700  
 701 specialized expertise. Imaging artifacts can arise from factors 701  
 702 such as tip contamination, especially in biological samples. 702  
 703 Only surface topology is directly accessible, whereas me- 703  
 704 chanical data require additional analysis. Finally, skin sam- 704  
 705 pling by tape stripping is sometimes difficult in patients with 705  
 706 damaged skin, and high-resolution throughput is relatively 706  
 707 low. 707

708 To address these limitations, various AFM technologies are 708  
 709 emerging. Low-cost, compact OPU-based AFMs could 709  
 710 enable point-of-care use. Hwu et al (XXX) are developing 710  
 711 user interfaces that allow a minimally trained user to produce 711  
 712 and analyze corneocyte images. High-speed mechanical 712  
 713 mapping through force–displacement scanning is being 713  
 714 implemented ([Liao et al, 2019](#)), and automated imaging 714  
 715 workflows and machine learning analysis will aid standard- 715  
 716 ization. These developments have the potential to make AFM 716  
 717 more accessible, streamlined, and informative. 717

718 Looking ahead, AFM has prospects for even greater impact 718  
 719 in dermatology, with significant potential to provide 719  
 720



nanoscale insights into skin health and disease. As a quantitative biomarker of skin barrier impairment, AFM could enable diagnostic screening, treatment selection, and therapeutic monitoring. Personalized medicine may be advanced by correlating nanotexture to genetic, immune, and molecular profiles in precision skin phenotyping. Beyond AD, AFM could provide insights into other inflammatory and age-related conditions affecting skin barrier and integrity. Point-of-care AFMs could allow rapid assessment during clinic visits to inform therapy.

## SUMMARY

SBF deregulations such as the ones found in AD have a significant and mounting impact on the well-being of the global population. In this review, we briefly described the anatomy involved with SBF. We introduced the use of AFM in dermatology and how it is used in scientific research to establish a quantitative *ex vivo* measurement by counting CNOs per unit area. We introduced the OPU-based AFM, a technology that can potentially make AFM-based measurements accessible to routine clinical applications. We reviewed a panel of articles that use corneocyte nanotexture to study the correlations between surface nanotexture and other parameters of skin health. We hope to show that AFM is a valuable tool in our understanding of dermatological diseases associated with impaired SBF, and we hope to motivate its adoption in clinical settings to provide caregivers and patients a powerful practical tool in the diagnosis and management of AD and other skin barrier dysfunctions.

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## CONFLICT OF INTEREST

The authors state no conflict of interest.

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Conceptualization: E-TH, JP; Funding Acquisition: E-TH; Investigation: JP, CMK, SK, MOC, SY, JPT, C-YC, CR, H-SL, BU, EG-Y, MH, E-TH; Methodology: JP, E-TH; Project Administration: E-TH; Supervision: CMK, SK, MOC, SY, JPT, C-YC, CR, H-SL, BU, EG-Y, MH, E-TH; Validation: CMK, SK, MOC, SY, JPT, C-YC, H-SL, BU, EG-Y, MH, E-TH; Writing – Original Draft Preparation: JP, E-TH; Writing – Review and Editing: CMK, SK, MOC, SY, JPT, C-YC, H-SL, IA, BU, EG-Y, MH, E-TH

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